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A bis-boronic acid modified electrode for the sensitive and selective determination of glucose concentrations
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A bis-boronic acid modified electrode for the sensitive and selective determination of glucose concentrations has been developed. The electrochemical characteristics of the sensor with added saccharides were investigated using cyclic voltammetry (CV) and electrochemical impedance spectroscopy (EIS). The bis-boronic acid modified electrode was both sensitive and selective for glucose.

Introduction

Saccharides such as D-glucose and D-fructose are important dietary sources of energy from natural carbohydrate sources and are used as processed food additives (high fructose corn syrup). From a clinical perspective measuring the concentration of D-glucose in blood is particularly important given the need of diabetic patients to regularly monitor its concentration, making fast and accurate determination of saccharides (particularly glucose) important. Many methods exist to measure the concentration of D-glucose including electrochemical and optical approaches. The most widely adopted sensors for D-glucose in food analysis, environmental monitoring, medical diagnosis, and many other fields are electrochemical in nature. Such saccharide sensors rely on the use of an enzyme such as glucose oxidase (GOx) or glucose dehydrogenase to generate redox mediator species, which are thereafter detected electrochemically. These sensors require the coupling of the enzyme in close proximity to the electrode in order to obtain high sensitivity. However, due to the intrinsic properties of enzymes, the catalytic activity of GOx is susceptible to environmental factors such as temperature, humidity, pH, ionic detergents, and toxic chemicals. Furthermore, GOx sensors suffer from high cost and poor stability and require complicated immobilisation procedures. Therefore, simple enzyme-free glucose sensing is highly desirable. Much work has been carried out in order to develop enzyme-free glucose sensors.

Enzymeless sensing is an important area of sensor development; robust, long shelf-life systems are required for use in the field. One approach towards enzyme-free sensors involves the direct oxidation of glucose at nanostructured electrodes. Nanostructuring allows the detection of glucose at a lower overpotential. However, such electrodes are very sensitive to adsorbed interferents such as chloride and suffer from surface fouling when used over prolonged periods. An alternative enzymeless approach for glucose detection involves the use of fully synthetic receptors, such as boronic acids. A boronic acid receptor binds reversibly with cis-1,2- and cis-1,3-diols to form five- and six-membered cyclic boronic esters, respectively. Boronic acid based receptors have been used successfully as fluorescence sensors, surface appended sensors, and potentiometric/amperometric sensors.

Among various analytical methods, electrochemical impedance spectroscopy (EIS) is an effective method to probe the interfacial properties of modified electrodes and is often used to probe chemical transformations and processes associated with conductive supports. EIS has been used in many fields, particularly corrosion, but only since 1980 has it become more widely applied, for ion-selective electrodes, electrochemical sensors and biosensors in general. EIS has been used to follow the chemical modification electrodes based on SAMs and to quantify species in solution. The recognition mechanism in these systems requires the blocking of electron transfer of a redox probe at the SAM/solution interface through complexation, and thus the species are recognised indirectly.

With our present work, an electrochemical sensor for saccharides has been prepared by surface modification of a gold electrode with a bis-boronic acid receptor. The receptor was designed to contain a glucose selective chemosensor unit (bis-boronic acid) and surface anchoring unit (sulphur), the
synthesis of which can be found in the ESI.† The selectivity of the sensors towards glucose, fructose, galactose and mannose was then evaluated using cyclic voltammetry (CV) and electrochemical impedance spectroscopy (EIS). As expected the sensor surface was particularly sensitive towards glucose. Our novel glucose selective bis-boronic acid designed for surface functionalisation has also been used in a partner paper that exploits surface plasmon resonance to detect the interactions between the bis-boronic acid functionalised surface and the different saccharides.‡

### Experimental

#### Materials

D-glucose, D-fructose, D-galactose, and D-mannose were purchased from Aladdin (Shanghai, China). Phosphate buffer solutions (PBS, pH 8.0) were prepared with 0.2 M NaH₂PO₄, 0.2 M Na₂HPO₄, and 0.1 M KNO₃. All other chemicals used were of analytical reagent grade and all solutions were prepared with deionised water obtained from a Milli-Q System (Millipore, USA).

#### Preparation of clean gold electrodes

Gold disk electrodes were polished with a 0.05 μm alumina slurry, cleaned by soaking in piranha solution (H₂SO₄ : H₂O₂ = 3 : 1) for 15 min, (Caution! Piranha solution should be handled with extreme care and should never be stored in a closed container. It is a very strong oxidant and reacts violently with most organic materials) and sonicated in water, twice. Then the electrode was electrochemically cycled from a potential of −1.0 to +1.25 V vs. Ag/AgCl in 0.5 M H₂SO₄ solution until a stable gold oxidation peak at 1.1 V vs. Ag/AgCl was observed.

#### Preparation of bis-boronic acid 1

Commercial bis(hexamethylene) triamine was reacted with (Boc)₂O to obtain a mono-boctriamine derivative. After reductive amination of pyrene carboxyaldehyde by this amine, the product can be converted to a Boc protected precursor to 1 by further alkylation with pinnacol protected 2-(bromomethyl)-phenyl boronic acid. The precursor upon deprotection with trifluoroacetic acid and reaction with the NHS ester of lipoic acid furnished bis-boronic acid 1 in 26% overall yield (five steps, Scheme 1). Compound 1 was synthesised by a modular approach allowing the potential incorporation of diverse functionalities to be delivered by this or future sensors (functionality dormant in one application may come to the fore in another). The chemosensor compound 1 includes a sulphur functionality for surface attachment. In this case we incorporate the known glucose selective bis-boronic acid unit to demonstrate the modular approach.

#### Preparation of the boronic acid modified gold electrodes

Gold electrodes were incubated in a solution of bis-boronic acid 1 in methanol (10 mM) for 2 days. The electrodes were rinsed with methanol and water, as represented in Scheme 2. Cyclic voltammetric measurements were performed using a CHI660C electrochemical workstation (Shanghai Chenhua, China). All electrochemical experiments were performed with a conventional three-electrode system, using the modified gold electrode (as shown in Scheme 2) as the working electrode, a platinum wire as the auxiliary electrode, and a saturated calomel electrode (SCE) as the reference electrode. Electrochemical impedance experiments were performed with a Zahner electrochemical workstation (Zahner, Germany) in PBS (pH 8.0) containing 5 mM Fe(CN)₆³⁻/⁴⁻ (1 : 1) with 0.1 M KNO₃. The impedance spectra were recorded within the frequency range of 10⁻¹ to 10⁷ Hz with an applied DC potential of 0.20 V and a sine wave potential of 10 mV. All potentials were reported with respect to the reference electrode. The ZSimpWin (Version 3.10) software was used to evaluate the experimental results of EIS.

#### Results and discussion

#### Electrochemical characteristics of the modified electrode

CVs at the bare gold electrode and the modified electrode in PBS (pH = 8.0) containing 5 mM Fe(CN)₆³⁻/⁴⁻ (1 : 1) with 0.1 M

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**Scheme 1** Structures of the starting material and product in the synthesis of bis-boronic acid 1 in five steps from N-1-(6-aminohexyl) hexane-1,6-diamine in 26% overall yield as detailed in the ESI.†

**Scheme 2** (a) Representation of gold surface functionalisation by receptor unit 1; and (b) saccharide binding.
the bis-boronic acid is immobilised on the gold electrode in a similar configuration to that depicted in Scheme 2.

The results obtained by EIS were verified using different electrical equivalent circuits shown in the inset of Fig. 1C. These circuits represented bare electrode (Fig. 1C-a, inset) and the modified electrode (Fig. 1C-b, inset) which were evaluated using ZsimpWin (Version 3.10) software. The EIS data were also simulated by the electrical equivalent circuit in Fig. 1C. We observed very good agreement between both experimental and calculated results from the best fitting electrical equivalent circuit model, where the chi-squared ($\chi^2$) value was minimized below $10^{-4}$. $\chi^2$ is the function defined as the sum of the squares of the residuals.

### The detection of saccharides by cyclic voltammetry (CV)

The electrochemical behaviour of the biosensor was then investigated using cyclic voltammetry. As shown in Fig. 2, the peak current decreases with increasing saccharide concentrations, and the peak-to-peak separation increases. We attribute this to the self-assembled layer on the gold electrode which acts as an inert electron transfer blocking layer. When the modified electrode is dipped into solutions of saccharides, the boronic acid binds with saccharides and further hinders the diffusion of the $\text{[Fe(CN)}_6^{3-/4-}$ toward the electrode surface. As shown in Scheme 2, when the bis-boronic acid interacts with saccharides, the effective surface area of the electrode is decreased, which limits the diffusion of the redox couple toward the electrode surface. This is rationalized from the curves in Fig. 2, in which $i_p$ with 1 mM $\text{D-glucose}$ is about 26.3 $\mu$A at pH 8.0 while that observed in the absence of $\text{D-glucose}$ is about 35.9 $\mu$A. Therefore, it is clear that $i_p$ decreases with increasing saccharide concentration.

Fig. 3 shows the peak current as a function of saccharide concentration, illustrating that the current versus concentration...
of saccharides gives a linear relationship between 0 and 10 μM. The stability constants reported previously using standard methods are:4 D-glucose (1.3 ± 0.3 × 10^5 M⁻¹), D-galactose (1.5 ± 0.2 × 10^5 M⁻¹), D-fructose (1.3 ± 0.3 × 10^4 M⁻¹) and D-mannose (6.5 ± 0.6 × 10^4 M⁻¹). The binding constants calculated are significantly higher than solution binding in exact value. These observed stability constants on the surface are also comparable in trend with that in the solution phase. The concentration limitation of the mathematical model and the disordering of the monolayer by binding reaction are both proposed to be the reasons (for details see the ESI†).

The detection of saccharides by electrochemical impedance spectroscopy

Electrochemical impedance spectroscopy is an effective method to investigate the interfacial properties of modified electrodes. The detailed information about the electric properties of the film on the modified electrodes could be acquired. Here, we demonstrate that impedance spectroscopy is a unique and sensitive technique in sensing the saccharides.

Fig. 4 shows the complex impedance plots of the bis-boronic acid modified electrode and after immersion in different concentrations of saccharides. Significant changes in the impedance spectra were observed for different concentrations of saccharides, the diameter of the semicircle parts increases with increasing saccharide concentration compared with the modified electrode, which shows that the complexation of the boronic acid group with saccharides changes the film characteristics, such as ion transfer resistance and the dielectric capacitance.

A modified Randle’s circuit (shown in Fig. 1C-b, inset) was used to fit the measured data. In this circuit, R₀ is the ohmic resistance due to an electrolyte and underlying electrode. Rct is the charge- and/or ion-transfer resistance occurring at the film/solution interface. The Warburg impedance represents semi-infinite linear diffusion within the solution. Since the interface between the electroactive film and the electrode is not a perfectly smooth plane but has some roughness and/or porosity, the ideal capacity is replaced by a frequency-dependent constant phase element (CPE), \( Z_{\text{CPE}} = Y_{0}(jω)^{-α} \) and \( α = 1 - ϕ \) (ϕ is equal to one for the complete smooth electrode).

The circuit element of most interest in this work is the charge-transfer resistance (Rct) which represents the charge- and/or ion-transfer resistance, because it often relates directly

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**Fig. 3** The calibration curve obtained using peak current as a function of saccharide concentration. The inset shows the linear relationship between the peak current and the concentration of saccharides applied in the calibration (from 0 to 10 μM).

**Fig. 4** EIS of the modified gold electrodes modified with a self-assembled monolayer of compound 1 with different concentrations of saccharides (from inner to outer: 0, 10^−6, 3 × 10^−6, 5 × 10^−6, 8 × 10^−6, 10^−5 M) in PBS (pH = 8.0) containing 5 mM Fe(CN)₆³⁻/⁴⁻ (1:1) with 0.1 M KNO₃. The frequency range is between 100 mHz and 100 kHz at the half-wave potential of 0.2 V with 10 mV sine wave potential.

**Fig. 5** Calibration curves obtained using Rct as a function of saccharide concentration. The frequency range is between 100 mHz and 100 kHz at the half-wave potential of 0.20 V with 10 mV sine wave potential. The inset shows the linear relationship between the Rct and the concentration of saccharides (from 0 to 10 μM).
to the accessibility of the modified electrode and reflects the flow of charge across the modified interface into the electrode. In this work, the $R_a$ of the self-assembled monolayer film increases with an increase in the saccharide concentration as shown in Fig. 5, indicating that the concentration of saccharides could be detected by monitoring changes in $R_a$. Saccharides are nonconductive therefore, the pathway of electrons or ions are blocked when saccharides bind with the bis-boronic acid on the modified electrode, and the electron/ion transfer resistance ($R_e$) increases with increasing saccharide concentration.

Fig. 5 shows the saccharide response curves of a modified electrode in PBS (pH 8.0), the change in ions are blocked when saccharides bind with the bis-boronic acid selectivity of the solution with expectations the absolute values calculated are significantly higher than those one might expect for a boronic acid–saccharide interaction alone. We expect the overall observed binding to be a consequence of the boronic acid receptor and saccharide interaction alone. We expect the overall observed binding to be a consequence of the boronic acid receptor and the electrochemical sensing regime used. Whilst remaining tentative, additional discussion is provided in the ESI† pertaining to the mathematical model and surface construction which might contribute to future discussion in this regard.

Conclusions

In this work, we have demonstrated that a surface modified gold electrode with a self-assembled monolayer of bis-boronic acid can detect four saccharides: d-glucose, d-fructose, d-galactose and α-mannose. Cyclic voltamograms and electrochemical impedance spectroscopy (EIS) were used to detect these four saccharides, and a very good linear response, high sensitivity and selectivity for glucose was achieved using this method.

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References


